

# Typical electrophysiological measurements and information they provide

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# Example: ion channel family in the Jurkat cells

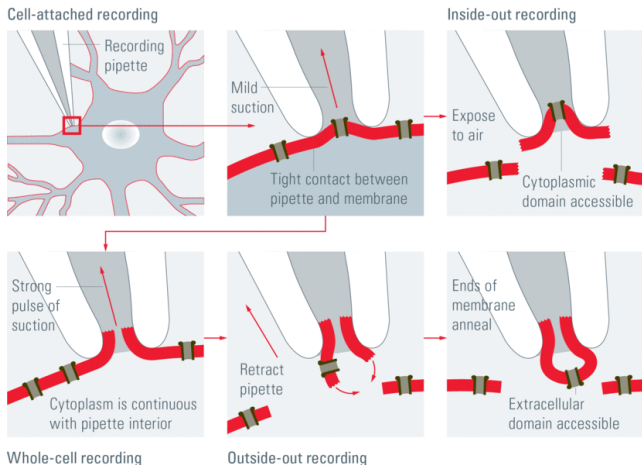
Channels (passive transporters)					
Channel	Selectivity	Conductance [pS]	Activation parameter	Function in Jurkat TL	Note
Kv1.3	K	3-5 (10-22?)	V (depolarization, Fig. 2, 2, 3)	V maintenance, Volume regulation	100-400 ICs/cell. main efflux pathway in T cells. Delayed rectifier. Unusually broad sensitivity to pharmacological agents. Raising [Ca], accelerates inactivation. Not the main pathway in our case [4].
KCa3.1	K	33-50	$Ca^{2+}$ , Fig. 2, 2, 3, Adenosine inhib [5]	V maint; T cell activation; cytokine production; autoimmune colitis	10-20 channels. Opens rapidly when $Ca^{2+}$ increases. [slow inactivation, delayed rectifier characteristics??]
Cl (mini)	Cl	1-2	Ca-activ?, (osmotic) pressure, hypotonic intra, ATP presence, swelling [2, 3, 6, 8]	Volume regulation	~ 10000 channels. Outward rectif. Current is induced with a ~ 1min delay following cell swelling, current is sustained as long as cytosolic ATP is present. $f \sim 300Hz$ . Average surface density 10-100 Cl channels/ $\mu m^2$ .
Cl (maxi)	Cl	300	V (hyperpolarisation)	Volume regulation	Time-dependent gating (inactivation). No evidence that these are activated by osmotic stress. [Lewis1993.Check!!!]
Cl	Cl	40	Ca, cAMP [9]	Volume regulation. Cytokine production by T cells?	No evidence that these are activated by osmotic stress. [Lewis1993.Check!!!]
	H ???		pH [10]		Speculative. Voltage increases by 47mV if $pH \rightarrow pH + 1$ ( $c_H \times 10$ )
TRPM4	Na, K, not Ca		$Ca^{2+}$ -activated, V-gated [2, 3]		
	Na		V		revealed by a small fraction (1-5%) of normal TL
TRPM7 (MIC)	Mg, Ca, K, Na		ATP enhanced. Mg, MgATP inhibited $Mg^{2+}$ depletion [2, 3]	Mg and Ca homeostasis during metabolic variations	Outward rectifying, nonspecific to mono- and divalent cations.
P2X <sub>7</sub>	Ca, Na, other cations?		ext ATP [11]	Ca homeostasis	
<i>Cav</i>	Ca		V [2]		debatable, not well documented
	Ca	~ 7	mitogen-stimulated [1][2]		$f^{-1} = 0.4 - 0.5s$ . Not measurably V-dependent.
CRAC	Ca	9-24 fS	$Ca^{2+}$ depletion in ER [2, 3]		low conductance, inward rectif
<i>IP<sub>3</sub>R</i> (in ER)	Ca		<i>IP<sub>3</sub></i>	Ca release from ER	In ER's membrane

# Example: ion channel family in the Jurkat cells

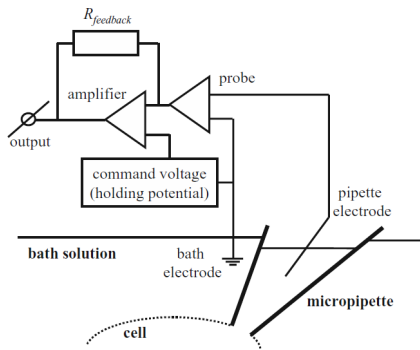
Pumps (active transporters)					
Na <sub>2</sub> /K-ATPase	Na <sub>2</sub> /K		ATP [13][14]	Na, K maintenance	3 Na out, 2 K in.
Plasma membrane Ca ATPase	Ca		ATP [15]	Ca extrusion from cytosol	
SERCA	Ca		ATP		Ca: from cytosol to the lumen of the ER
Proton pump	H		ATP (exist in our case???)		H out
Exchangers (secondary active transport)					
Na/H	Na, H		ATP regulated [16][18]	major $pH_i$ regul. Cellular vol	
Cl/ HCO <sub>3</sub>	Cl, HCO <sub>3</sub>		[18]	Volume regul	
Na <sub>2</sub> /K/2Cl cotransporter	Na, K, 2Cl		??? [18]	Volume regul	Na:K:2Cl. Energy from Na-EiChem grad (secondary active transport)
Other conductors					
Aquaporin	H <sub>2</sub> O		[19]		
GLUT-1	glucose		[20][21]	glucose transport effector	
Pannexin-1	ATP		[22]	T-cell activation at the immune synapse	

# Patch-clamp: major electrophysiological tool

- 1 Whole-cell
- 2 Perforated patch
- 3 Cell-attached
- 4 Loose patch
- 5 Inside-out patch
- 6 Outside-out



# Whole-cell patch-clamp technique



Chemical	ECS concentration (mM)	ICS concentration (mM)
Na <sup>+</sup>	126	5
K <sup>+</sup>	6	147
Mg <sup>2+</sup>	2.5	1.2
Ca <sup>2+</sup>	1.2	0
Cl <sup>-</sup>	125	150
GTP	0	0.1
ATP	0	5
HEPES	10	20
Glucose	11	11
Sucrose	67	0

# Properties

## Peculiarities:

- 1 large pipette
- 2  $V_b \gg V_p \gg V_c$
- 3 perfusion
- 4 Dialysis

## Assumptions:

- 1 Constant temperature
- 2 Equal osmolarities
- 3 Equal pH
- 4 Equal hydraulic pressure
- 5 No hardware filtering

## Advantages:

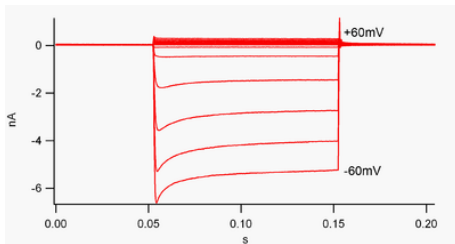
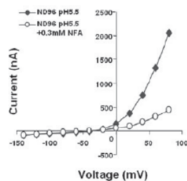
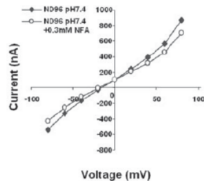
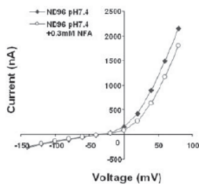
- 1 Quick assertion of ion channel populations
- 2 Cytosolic environment is controlled
- 3 Extracellular side can be perfused

Disadvantage: Washout of cytosolic factors (Dialysis).

Separation of required current:

- ① Shape of the current response
- ② Drugs (blockers for specific channels and pumps)
- ③ Manipulation of ion concentration. Problem with an unknown channel.

# Conductance

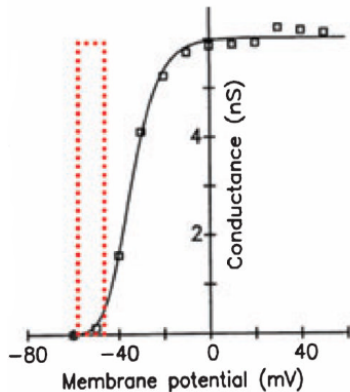




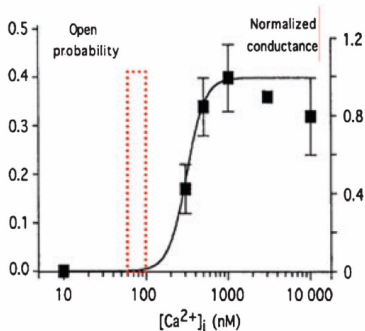
# Conductance

$f(V)$  or  $f(\text{Ca}, \text{etc})$

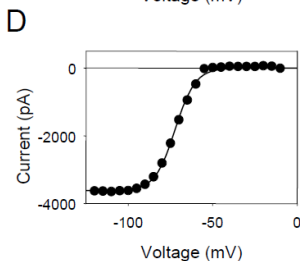
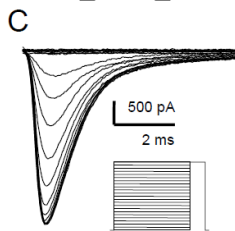
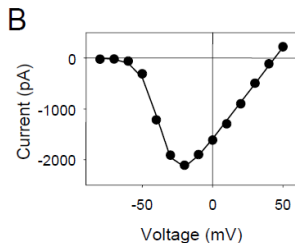
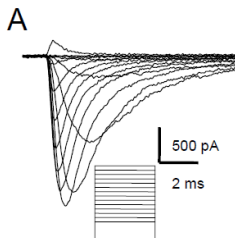
### Voltage dependence



### Calcium dependence

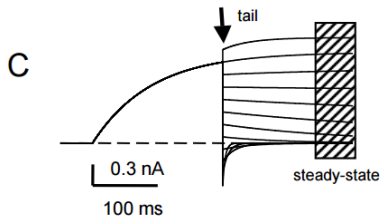
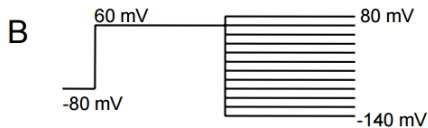


# Peak currents



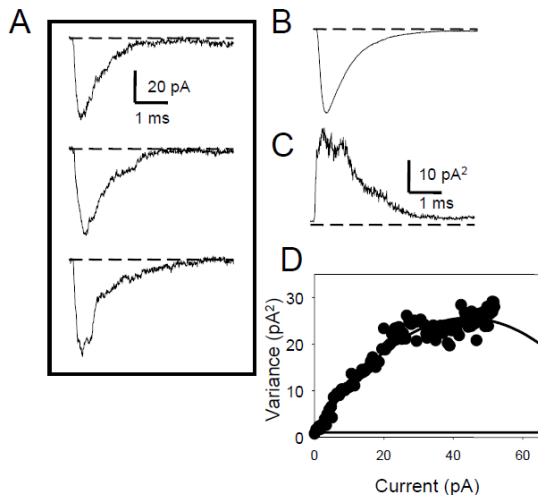
$$I(V) = G_{Na}(V - E^{rev}) \frac{1}{1 + \exp[z_g(V_{1/2} - V)F/RT]}$$

# Tail-current analysis



Equilibrium (Nernst) potential:  $E^{rev} = \frac{RT}{zF} \ln\left(\frac{c^e}{c^i}\right)$

# Non-stationary noise analysis



$$I(t) = \sum a_m e^{-t/\tau}$$

$$\sigma^2 = iI - I^2/N$$

# Single-channel recordings



conduction

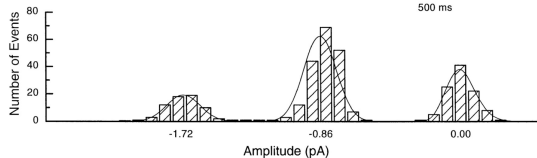
rectification

dwelt time (open probability)

**A**



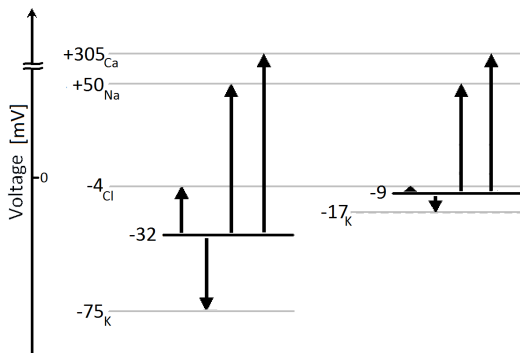
**B**



# GHK: V(C)

Easy and therefore common

$$\phi = \frac{RT}{F} \ln \left[ \frac{P_K c_K^e + P_{Na} c_{Na}^e + P_{Cl} c_{Cl}^i}{P_K c_K^i + P_{Na} c_{Na}^i + P_{Cl} c_{Cl}^e} \right],$$



## Assumptions:

- 1 constant electric field
- 2 ions move under the influence of diffusion and the electric field
- 3 concentrations of ions at the edges of the membrane are directly proportional to those in the aqueous solutions.
- 4 The ions access the membrane instantaneously from the intra- and extracellular solutions.
- 5 The membrane is a homogeneous substance
- 6 The permeant ions do not interact.

## Disadvantages:

- 1 Constant field contradicts Poisson's eq.
- 2 Steady. Fixed bulk concentrations.

# Phenomenological models

Polynomial equations to describe ionic current kinetics

Functions are more intimately associated with physical realities

Many parameters (usually obtained from experimental fit)

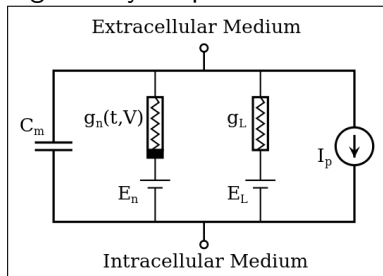
HH

FitzHugh-Nagumo



# Hodgkin-Huxley model

Ingenuously simple.



$$I = I_p + C_m \frac{dV_m}{dt} + \bar{g}_K n^4 (V_m - V_K) + \bar{g}_{Na} m^3 h (V_m - V_{Na}) + \bar{g}_l (V_m - V_l),$$
$$\frac{dn}{dt} = \alpha_n(V_m)(1 - n) - \beta_n(V_m)n$$
$$\frac{dm}{dt} = \alpha_m(V_m)(1 - m) - \beta_m(V_m)m$$
$$\frac{dh}{dt} = \alpha_h(V_m)(1 - h) - \beta_h(V_m)h$$

# HH: pros and cons

Current balance equation obtained using Kirchoff's law and relaxation equations for the components in the ionic conductances.

Accurate assumption:  $K_v^+$  channels contain four identical voltage-sensor domains that can activate largely independently.

Assumptions:

- Ionic currents obey Ohm's law
- The channel contains four independent and identical voltage sensors that activate in two steps.
- Channel opening (CO) represents a concerted conformational change that follows but is distinct from voltage-sensor activation.

Limitation:

Does not capture correctly the kinetics of the  $Na^+$  channel.

Cannot account for the stochastic response to current injection (discrete nature of ion channels).

Spatial domain effects

Hydration

No C-V coupling

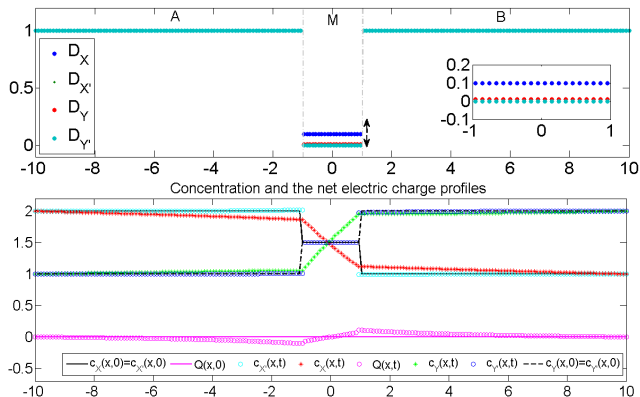
- How the activity of ion channels alters voltage properties?
- Why do fluctuations appear?
- What defines their magnitude?
- How the observed spectrum can be explained?

Briefly: theory is needed.

# Simple model: Poisson-Nernst-Planck

$$\frac{\partial c_m}{\partial t} = -\nabla \mathbf{J}_m, \quad \mathbf{J}_m = -D_m \left( \nabla c_m - \frac{z_m e}{k_B T} c_m \mathbf{E} \right) + \mathbf{j}_m,$$

$$\nabla \varepsilon \mathbf{E} = -\nabla(\varepsilon \nabla \phi) = 4\pi \rho = 4\pi e \sum_m z_m c_m,$$



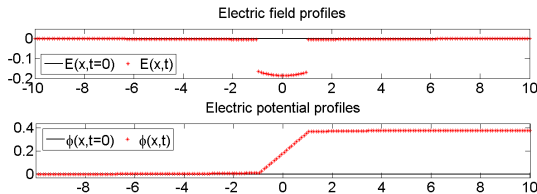
# PNP: Pros and cons

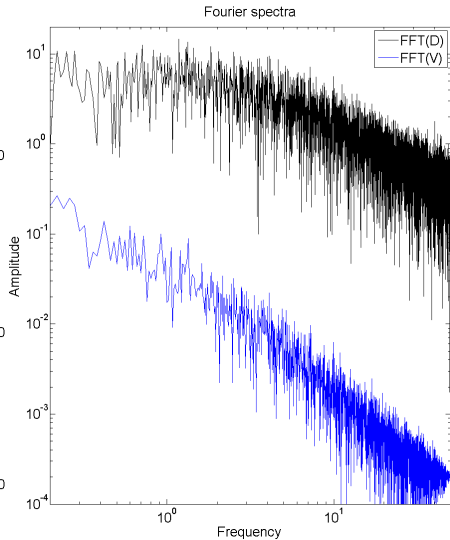
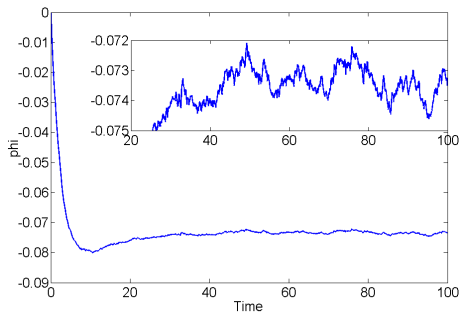
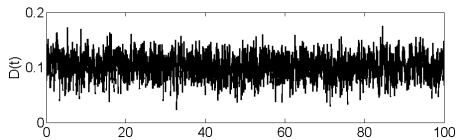
## Advantages:

- 1 from profound physical principles
- 2 self-consistent
- 3 computationally cheap
- 4 I-V curves. Detection of a given ion species.

## Faults:

- 1 Continuous. Not applicable in narrow channels.
- 2 No saturation
- 3 No self-energy barrier
- 4 Spontaneous gating only. No voltage gating.





# PNP: main result

