MGH/HST Athinoula A. Martinos Center for Biomedical Imaging





Reconstructing multivariate causal structure between functional brain networks through a new Laguerredecomposition based Granger causality approach

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From Correlation to Causation



- functional brain connectivity: statistical dependencies among nonspatially-contiguous neuro-physiological events.
- fMRI correlation studies provides important insight





Limitations in fMRI

Local variations in HRF parameters

- Inter-regional differences in haemodynamic response function might obfuscate underlying neural dynamics
- Signal not very suitable: need to find a tradeoff between SNR and TR (sampling frequency)
- short signals, and too many parameters



- Turns out that GC is **invariant to haemodynamic convolution** (Deshpande 2010, Shippers 2011, Barnett, 2011, Seth 2013)
- However, GC is sensitive to sampling frequency and/or eccessively low SNR (*seth 2013*)
- Problem in principle becomes "only" problem in practice (which could be tackled with technology)
- Use of "blind deconvolution approach" for resting state? [Wu et al, Medical Image Analysis (2013)]

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$$X_{t} = \sum_{k=1}^{p} A'_{k} X_{t-k} + \sum_{k=1}^{p} B'_{k} Y_{t-k} + \varepsilon'_{t}$$

$$X_{t} = \sum_{k=1}^{p} A_{k} X_{t-k} + \sum_{k=1}^{p} B_{k} Y_{t-k} + \sum_{k=1}^{p} C_{k} Z_{t-k} + \varepsilon_{t}$$

We want to "search" into the past but we can't afford a large autoregressive order.

Squeeze more "past" per parameter!

$$x_{t} = \mathbf{A} \left(\mathscr{L}^{(m)}(x) \oplus \mathscr{L}^{(m)}(z) \right) + \varepsilon_{t}$$

$$x_{t} = \mathbf{A}' \left(\mathscr{L}^{(m)}(x) \oplus \mathscr{L}^{(m)}(y) \oplus \mathscr{L}^{(m)}(z) \right) + \varepsilon_{t}'$$

$$\mathscr{L}^{(m)}(x) = \sum_{n=1}^{N} (\phi_m)(x_{N-n} - x_{N-n-1})$$

$$\bullet \phi_m(n) = \alpha^{\frac{n-m}{2}} (1-\alpha)^{\frac{1}{2}} \sum_{j=0}^m (-1)^j \binom{n}{j} \binom{m}{j} \alpha^{m-j} (1-\alpha)^j$$

Laguerre polynomials

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 ϕ_0

 ϕ_1

 ϕ_3

 ϕ_4

 ϕ_{5}

 $\phi_2 \otimes$

input signal

naw

 \mathcal{L}_{0} \mathcal{L}_{1} $\mathcal{L}_{2} =$ \mathcal{L}_{3} \mathcal{L}_{4}

Laguerre-based Granger causality

Synthetic simulations

Several network topologies





• Characterization of sensitivity and specificity





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$$\overset{\mathcal{L}_0}{\longleftarrow} \qquad \overset{\phi_0}{\longleftarrow} \qquad \overset{\text{input signal}}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\text{input signal}}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_3}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_1}{\longleftarrow} \qquad \overset{\phi_2}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_4}{\longleftarrow} \qquad \overset{\phi_5}{\longleftarrow} \qquad \overset{\phi_6}{\longleftarrow} \qquad \overset{\phi$$







800+ subjects (age 28 ± 3) scanned Single-shot 2D EPI readout TR =0.72 s, whole brain coverage



Networks definitions by ICA components:



- Subject-level ICA+FIX (physiological noise removal)
- Group-level: Group-PCA (Melodic's incremental)
- Subject-level: Group-ICA (at 15,25,50 components)

Each ICA component signal is an average of a 3D-volume

+ deconvolution for HRF influence removal



Networks definitions by ICA components:





- 450+ subjects analysed
- Results extremely stable; qualitative same results for:
 - small changes of autoregressive order
 - small changes of α -parameter
 - with or without HRF deconvoltion
- Almost hierarchical topology

Neurophysiological interpretation

	ICA neurological meaning
1	Secondary Visual network (extrastriate visual network)
2	Default Mode Network (DMN)
3	Primary Visual network (striate visual network)
4	Visuo-premotor network
5	Fronto-Parieto-Cerebellar network left side
6	Fronto-Parieto-Cerebellar network right side
7	Salience network (SN)
8	Basal Ganglia visual striate network including dmPFC (mainly)
9	Cerebellar network
10	Hippocampal,
	medial temporal lobe memory spatial orientation network
11	Sensory-motor network
12	Fronto-temporal-parietal "language" network
13	no unique neurophysiological interpretation
14	Fronto-polar-higher executive function network
15	no unique neurophysiological interpretation



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Neurophysiological interpretation

- The default-mode-network (DMN) modulate the salience-network (SN)
 We demonstrate for the first time that this interaction may be driven by topdown signal from the DMN to SN
- DMN "top-down" influence on frontotemporal circuits localized across regions strongly implicated in language production, comprehension and semantic memory. DMN top-down inputs to the extended frontotemporal language network as the basis of the linguistic self-referential processes (thought to enhance the consciousness experience).

Conclusions

- Laguerre-based GC delivers better performance as compared to classical, linear MVAR-based Granger causality methods.
- Laguerre-based GC applied detect in vivo functional interactions and causal dynamics across multiple neural networks

Future work

• Investigation of information flow between in vivo functional networks during specific-task (cognitive, memory, sensory, motor, etc...).

